

# Formulation And Evaluation Of Controlled - Release Floating Tablets Of Pregabalin

Supriya Udayagiri\*, C.Meenakshi, R.Gnanamayee, K.Manasa, S.Sindhu, M.Deva,  
B.Nagendrababu, N.Nrupavani

## Abstract:

The present study focuses on the formulation and evaluation of controlled release floating tablets of Pregabalin to enhance its gastric retention time and provide sustained drug release, thereby improving therapeutic efficacy and patient compliance. Pregabalin, a widely used antiepileptic and neuropathic pain-relieving agent, has a short half-life and requires frequent dosing. To address these limitations, floating drug delivery systems (FDDS) were developed using hydrophilic polymers such as Hydroxypropyl Methylcellulose (HPMC K4M/K15M), Carbopol 934P, and Xanthan gum, in combination with gas-generating agents like sodium bicarbonate and citric acid. The tablets were prepared by direct compression and evaluated for pre-compression and post-compression parameters including hardness, friability, weight variation, drug content, floating lag time, total floating time, swelling index, and in vitro drug release. Dissolution studies were conducted in 0.1 N HCl (pH 1.2) to simulate gastric conditions, and the drug release data were analyzed using various kinetic models to determine the release mechanism. The results suggest that the developed floating tablets of Pregabalin offer a promising controlled release system capable of improving bioavailability and reducing dosing frequency.

**Keywords:** Pregabalin, floating tablets, controlled release, FDDS, HPMC, drug release kinetics, gastroretentive system.

## 1.Introduction:

Oral delivery of drugs is the most preferable route among all the drug delivery due to the ease of administration, patient compliance and flexibility in formulation. From immediate release to site specific delivery, oral dosage forms have really progressed. The goal of any drug delivery system is to provide a therapeutic amount of the drug to the proper site in the body to achieve promptly, and then maintain, the desired drug concentration. Technological attempts have been made in the pharmaceutical research and development of rate-controlled oral drug delivery systems to overcome physiological adversities, such as short gastric residence times (GRT) and unpredictable gastric emptying times (GET). Dosage forms that can be retained in the stomach are called Gastro retentive drug delivery systems (GRDDS). GRDDS can improve the controlled delivery of drugs that have an absorption window by continuously releasing the drug for a prolonged period of time before it reaches its absorption site, thus ensuring its optimal Bioavailability. Invariably, conventional dosage forms do not maintain the drug blood levels within

the therapeutic range for an extended period of time. To achieve the same, a drug may be administered repeatedly using a fixed dosing interval. This causes several potential problems like saw tooth kinetics characterized by large peaks and troughs in the drug concentration-time curve

### 1.1. Limitations of floating GRDDS

One of the major disadvantages of floating systems is the requirement of high levels of fluids in the stomach for the delivery system to float and work efficiently. These systems also require the presence of food to delay their gastric emptying. In addition, there are limitations to the applicability of floating systems for drugs that have solubility or stability problems in the highly acidic gastric environment or that are irritants to the gastric mucosa.

Furthermore, the relatively brief gastric emptying time in humans, which normally averages 2-3 hrs through the major absorption zone (stomach or upper part of the intestine), can result in incomplete drug release from the DDS leading to diminished efficacy of the administered dose. Thus placement of the DDS in a specific region of the GIT offers numerous advantages, especially to the drugs having narrow absorption window in GIT, primarily absorption in the stomach, stability problems in intestine, poor solubility at alkaline pH, local activity in stomach, and property to degrade in colon. It has been suggested that compounding the drugs with narrow absorption window in a dosage form, which prolongs the gastric residence time would an extended absorption phase of these drugs.

### 1.2. Sustained Drug Delivery:

Floating systems can remain in the stomach for longer period and hence can release the drug over a prolonged period of time. The problem of short gastric residence time encountered with an oral CR formulation hence can be overcome with these systems. These systems have a bulk density of GI as a result of which they can float on the gastric contents.

### 1.3. Absorption Enhancement:

Drugs that have poor bioavailability because of site specific absorption from the upper part of the gastrointestinal tract are potential candidates to be formulated as floating drug delivery systems, thereby maximizing their absorption. In developed a multiparticulate system that consisted of floating pills of a drug (p- amino benzoic acid) having a limited absorption site in the gastrointestinal tract. It was found to have 1.61 times greater AUC than the control pills (Ichikawa et al). FDDS also serves as an excellent drug delivery system for the eradication of *Helicobacter pylori*, which causes chronic gastritis and peptic ulcers. The treatment requires high drug concentrations to be maintained at the site of infection that is within the gastric mucosa. By virtue of its floating ability these dosage forms can be retained in the gastric region for a prolonged period so that the drug can be targeted.

#### 1.4. Muco-adhesive systems:

The concept of Mucoadhesive (or bioadhesive) systems is that an oral dosage form in the stomach can stick to the mucosal surface of gastric tissue. Once the dosage form firmly sticks to the mucosal surface, its gastric residence time is expected to be prolonged until it is removed by turnover of mucin. It is a simple and yet highly innovative concept.

#### 1.5. Advantages of mucoadhesive system

Permits localization of the drug at the absorption site for a prolonged period of time.

1. A significant reduction in dose can be achieved, increasing patient compliance.
2. Drugs, which show poor bioavailability, can be administered conveniently.
3. It reduces dose dependent side effects due to lowering of frequency of drug dosing.

#### 1.6. Limitations of mucoadhesive system:

1. Drugs which irritate the mucosa cannot be administered by this route.
2. Drugs which are unstable at gastrointestinal pH cannot be administered by this route.
3. Only low dose drugs can be administered.
4. Over hydration may lead to formation of slippery surface disrupting the structural integrity of the formulation by swelling and hydration of the bioadhesive polymers.

Gastroretentive drug delivery system is an approach to prolong gastric residence time, thereby targeting site specific drug release in upper gastrointestinal (GI) tract. Floating drug delivery system (FDDS) and bioadhesive drug delivery are widely used techniques for gastro retention (Singh and Kim, 2000). We will elaborate the most important features of the core research pursued on the above mentioned subject. The following chapter gives the review of literature in the light of subject discussed here.

#### 1.7. Criteria for Selection of Drug Candidate for GRDDS:

Drugs required to exert local therapeutic action in the stomach

e.g. Misoprostol, 5-Fluorouracil, antacids and anti-reflux preparations, anti-*Helicobacter pylori* agents and certain enzymes.

1. Drugs exhibiting site-specific absorption in the stomach or upper part of the small intestine:

e.g. Atenolol, Furosemide, Levodopa, *p*-Aminobenzoic acid, Piretanide, Salbutamol.

2. Drugs unstable in lower part of GI tract:

e.g. Captopril.

3. Drugs insoluble in intestinal fluids (acid soluble basic drugs):

e.g. Chlordiazepoxide, Chlorpheniramine, Cinnarizine, Dizapam, Diltiazem, Metoprolol,

Propranolol, Verapamil.

4. Drugs with variable bioavailability:

e.g. Sotalol hydrochloride and Levodopa.

## 2. Aim & Objective:

Gastro retentive controlled release systems provide drug release in an amount sufficient to maintain the therapeutic drug level over an extended period of time. The real challenge in the development of an oral controlled release drug delivery system is not just to sustain the drug release but also to prolong the presence of the dosage form within the gastrointestinal tract (GIT) until all the drug is completely released at the desired period of time. The objective of the present research work was to prepare and evaluate controlled- release floating tablets of pregabalin that can be floated in the stomach, so that the gastric residence time is increased thus prolonging the drug release and improve oral bioavailability by using various gelling polymers such as Hydroxypropyl methyl cellulose.

Pregabalin (PGB), a gabapentinoid drug, is widely used in diabetic neuropathy, post-herpetic neuralgia, fibromyalgia and partial-onset seizures. Pregabalin has not been absorbed equally by GIT. It mainly absorbs from the upper GIT. Pregabalin has a short half-life, whereby the conventional pregabalin capsule available in the market is administered two to three times a day. Therefore to reduce the dosing frequency of pregabalin need a gastroretentive controlled release system. Therefore it was decided to formulate and evaluate controlled- release floating tablets of pregabalin using different combination of HPMC K4M and HPMC K100LV.

## 3. Plan of Work:

- Selection and procurement of drug, polymer and excipients.
- Preformulation studies.
- Compatibility study of drug with different polymers and excipients.
- Formulation of floating dosage form.
- *In vitro* evaluation of formulated floating dosage form.
- Stability studies on floating dosage form as per ICH guidelines.

#### 4. Materials and Methods:

##### Materials

The following drug, excipients and chemicals were used for the formulation and evaluation of Gastroretentive drug delivery system.

**Table 3:** List of drugs, polymers, excipients, chemical and reagent used for study

Drug	Name of Manufacturer
Pregabalin	Drugs India, Hyd
<b>Polymers and Excipients</b>	
HPMC (K4M, K100 LV)	Colorcon Asia Pvt. Ltd., Goa, India
Microcrystalline cellulose (MCC KG 100)	S.D. Fine Chemicals., Mumbai, India
Sodium bicarbonate	Lubrizol., Mumbai, India
Anhydrous citric acid,	S.D. Fine Chemicals., Mumbai, India
Magnesium stearate	S.D. Fine Chemicals., Mumbai, India
Talc	S.D. Fine Chemicals., Mumbai, India
<b>Reagents</b>	
(1) Acetonitrile (HPLC grade)	Merck Specialties Pvt. Ltd.
(2) Disodium dihydrogen orthophosphate	Loba chem.
(3) Orthophosphoric acid (AR grade)	Merck Specialties Pvt. Ltd.
(4) Tetrabutylammonium hydroxide	Loba chem.
(5) Water (HPLC grade or equivalent)	Milli Q.

**Table 4:** List of Equipment's, make and model used for the study**4.2. Methodology:****1. Preformulation study:****A) Identification of drug**

Identification of drug was carried out by infrared spectroscopy and differential scanning calorimetry (DSC).

Equipment's Name	Name of Manufacturer and Model
Digital Balance	AUX 120, Shimadzu, Japan.
Differential scanning calorimeter	METTLER DSC 30 S, Mettler Toledo India Pvt. Ltd.
Infra Red Spectrophotometer KBr Press	8400S, Shimadzu, Kyoto Japan. KBr press, TSI, Mumbai Electrolab ETD 1020, Mumbai, India. Electrolab TDT 08 L Plus.
Tap density tester USP II Dissolution Test Apparatus Disintegration apparatus Sonicator	Electrolab, disintegration tester (USP) ED-2L LAB-HOSP, Mumbai
Digital pH meter Stability chamber	Elico Model- LI 612 CHM-10S Remi Lab, Mumbai.
Tablet compression machine HPLC	Rimek minipress-1, Ahmedabad, India. Agilent technologies.
Hardness tester Vernier caliper X-ray machine Roche friabilator	Monsanto hardness tester. Mitutoyo, Absolute, USA. Wipro GE DX-300, Pune, India.
Ultraviolet Spectrophotometer Mechanical stirrer Mucoadhesive strength determination Apparatus	Electrolab, EF-2, Friabilator (USP). Shimadzu 1700, Japan Remi Instruments, Mumbai, India. Fabricated in lab.

**2. Infrared spectroscopy:**

The potassium bromide disk method was used for the preparation of sample. IR spectrum of drug was measured in the solid state as potassium bromide dispersion. The bands ( $\text{cm}^{-1}$ ) have been assigned.

**3. Differential scanning calorimetry study:**

Melting point of drug was determined by using DSC. The drug was hermetically sealed in perforated aluminum pans and heated at constant rate of  $10^{\circ}\text{C} / \text{min}$  over the temperature ranges of

50-300 °C.

### **B) Melting point determination:**

The melting point of Pregabalin were determined by using melting point apparatus.

### **C) Solubility study of Pregabalin in different solvents:**

The solubility of drug to be determined by taking 10 ml of various medium and then cumulative addition of drug was carried out in order to make saturated drug solution, maintained at  $37\text{ }^{\circ}\text{C} \pm 0.5\text{ }^{\circ}\text{C}$  in a water bath and continually shaken in to mechanical shaker (Remi mechanical shaker, Mumbai) up to 24 h. Samples were withdrawn, filtered through a filter paper (pore size  $0.45\text{ }\mu\text{m}$ ), suitably diluted and assayed by UV spectrophotometer.

### **D) Standard calibration curve**

#### **4.3. Standard calibration curve of Pregabalin in pH 3 buffer:**

Stock standard solution was prepared by dissolving accurately weighed 100 mg Pregabalin in volumetric flasks, dissolved in methanol and diluted to 100 ml with freshly prepared in glycine buffer (pH 3.0). The stock solution was filtered through a  $0.45\text{ }\mu\text{m}$  membrane filter. A standard curve was prepared by withdrawing appropriate aliquots from stock solution into a series of 10 ml of volumetric flasks. The volume was made upto the mark with mobile phase to obtain concentration range 10-20  $\mu\text{g/ml}$  of Pregabalin. Detection of Pregabalin was performed with the UV spectrophotometry set at 226 nm. Peak area was recorded and calibration curves were plotted with peak area verses the respective concentration of Pregabalin.

**E) Evaluation of precompression parameters of drug, polymer and excipients** Drug, polymers and excipients were characterized for their physical properties such as angle of repose, density, compressibility, Hausner's ratio. Pregabalin and Pregabalin were evaluated for particle size determination by Malvern technique.

#### **4.4. Angle of Repose:**

The frictional forces in a loose powder or granules can be measured by the angle of repose. This is the maximum angle possible between the surfaces of a pile of powder or granules and the horizontal plane. Different ranges of flow ability in terms of angle of repose shown in Table 5. The angle of repose was determined by the funnel method (Lachman et al., 1990, V. Bhavani et al., 2012). The accurately weighed powder was taken in a funnel. The height of the funnel was adjusted in such a way that the tip of the funnel just touched the apex of the heap of the powder. The powder was allowed to flow through the funnel freely onto the surface. The diameter of the powder cone was measured by scale. The angle of repose was calculated using the following equation.

$$\tan(\Theta) = h / r \quad (1)$$

Where 'h' and 'r' are the height and radius respectively of the powder cone

**Table 5:** Different ranges of flow ability in terms of angle of repose:

Angle of repose, ( $\Theta$ )	Predicted flow property
< 25	Excellent
25-30	Good
30-40	Passable
>40	Very poor

#### 4.5. Determination of bulk density:

Weigh accurately 25 gm of material (W), which was previously passed through 20 # sieve and transfer in 100 ml graduated cylinder. Carefully level the powder without compacting, and read the unsettled apparent volume ( $V_0$ ) (USP., 2010). Calculate the apparent bulk density in gm/ml by the following formula.

$$\text{Bulk density} = \text{Weight of powder} / \text{Bulk volume} \quad (2)$$

#### 4.6. Determination of tapped bulk density:

Tapped bulk density is the ratio of weight of the powder sample to its tapped volume. Weigh accurately 25 gm of material, which was previously passed through 20 # sieve and transfer in 100 ml graduated cylinder. Then mechanically tap the cylinder containing the sample by raising the cylinder and allowing it to drop under its own weight using mechanically tapped density tester that provides a fixed drop of  $14 \pm 2$  mm at a nominal rate of 300 drops per minute. Tap the cylinder for 500 times initially and measure the tapped volume ( $V_1$ ) to the nearest graduated units, repeat the tapping an additional 750 times and measure the tapped volume ( $V_2$ ) to the nearest graduated units. If the difference between the two volume is less than 2 % then final the volume ( $V_2$ ) (USP., 2010).

$$\text{Tapped Density} = \text{Weight of powder} / \text{Tapped Volume} \quad (3)$$

#### 4.7. Compressibility index:

The compressibility index of material was determined by following equation (Reddy *et al.* 2003).

$$\text{Carr's Index} = [(\text{Tapped bulk density} - \text{Loosed bulk density}) \times 100 / \text{Tapped bulk density}] \quad (4)$$

#### 4.8. Hausner's ratio:

Hausner's ratio was determined by following equation (Lachman *et al.*, 1990) Hausner's ration = Tapped bulk density / Loosed bulk density (5) **Table 6:** Standard values of Carr's index and Hausner's ratio

Carr's index	Type of flow	Hausner's Ratio
<10	Excellent	1.00-1.11
11-15	Good	1.12-1.18
16-20	Fair	1.19-1.25
21-25	Passable	1.26-1.34
26-31	Poor	1.35-1.45
32-38	Very poor	1.46-1.59
>38	Very, Very poor	>1.60

#### F) Particle size determination

Particle size determination of Pregabalin was determined using dry method by Malvern technique.

#### G) Drug excipients compatibility study

The drug excipients interaction study was carried out by using Fourier transform infrared spectroscopy and Differential scanning calorimetry.

#### 4.9. Differential scanning calorimetry study:

Physical mixtures of drug and drug with excipients were filled in dried vial. The sealed vials were stored at 40 °C/ 75 % RH for four weeks in stability chamber. At the end of four weeks vials were removed from stability chamber and subjected for interaction study. Drug polymer interaction study was carried out by using DSC. In this study thermogram of pure drug, drug with polymer and mixtures of drug with excipients were taken. Heating was done at a scan rate of 10 °C / min. over a temperature range of 30 to 340 °C in a dynamic Nitrogen atmosphere. An empty sealed Aluminum pan was used as a reference.

#### 4.10. FTIR spectroscopy study:

IR spectroscopy was used to determine the molecular interaction between drug and excipients. The above (as per DSC study) all physical mixtures and drug sample were mixed with dried KBr in ratio 1:100. The mixture was compressed to a 12 mm semi transparent disk by applying a pressure of 10 tons for 2 min. The FTIR spectra over the wavelength range 4000-400 cm<sup>-1</sup> were recorded using a FTIR spectrometer (8400S, Shimadzu, Japan).

#### 4.11. Pregabalin Gastroretentive drug delivery system:

In the present study, statistical experimental design was used in order to get more information about the effect of formulation components on drug release and to obtain the optimum formulation through minimum time and expenses. The levels of the two factors were selected on the basis of preliminary studies carried out before implementing the experimental design. The experimental design was generated using state-of-art computerized optimization software Design Expert Version 8.0.3.1

(Design Expert, 2010).

#### 4.12. Experimental Design (For Floating Gastroretentive drug delivery system):

In

$3^2$  full factorial design, 2 independent variables Polymer 1 are Concentration of HPMC K4M / HPMC K4M (P1) and Polymer 2 are Concentration of HPMC K100LV (P2) were selected at 3 different levels for, Percentage drug release at 12 h (Q 12), Total floating time (TFT), Buoyancy lag time, as dependent variables (Table 7). Experimental trials were performed using all 9 possible combinations were shown in Table 10-11(Design Expert Version 8.0.3..1).

**Table 7:** The variables used in Gastroretentive Floating tablets of Pregabalin

Independent variables	Symbols	Dependent variables
Concentration of HPMC K4M / HPMC K4M	P1	% Drug released (Q 12) Total floating time (TFT) Buoyancy lag time (BLT)
Concentration of HPMC K100 LV	P2	

#### 4.13. Preparation of Gastroretentive tablets of Pregabalin:

Pregabalin tablets were prepared by the direct compression method. Each tablet contained about 330 mg of the drug. All the ingredients were sifted through sieve no. 40 and magnesium stearate was passed through sieve no 60. The required quantities of the materials were mixed thoroughly for 15 minutes in polybag and lubricated with magnesium stearate for 3 minutes.

Compositions of all the formulation were given in Table 8

**Table 8:** Composition of Pregabalin Floating tablets (X1-X9)

Ingredients (in mg)	X1	X2	X3	X4	X5	X6	X7	X8	X9
Pregabalin	330	330	330	330	330	330	330	330	330
HPMC K4M	16.5	21.45	26.40	16.5	21.45	26.40	16.50	21.45	26.40
HPMCK100 LV	26.40	26.40	26.40	33.0	33.0	33.0	39.60	39.60	39.60
MCC KG-100	21.55	16.60	11.65	14.95	10.0	5.05	8.35	3.40	3.45
Sodium lauryl sulphate	4.90	4.90	4.90	4.90	4.90	4.90	4.90	4.90	4.90
Citric acid	14.70	14.70	14.70	14.70	14.7	14.7	14.70	14.70	14.70

					0	0			
Sodium bicarbonate	73.50	73.50	73.50	73.50	73.50	73.50	73.50	73.50	73.50
Magnesium stearate	2.45		2.45	2.45					
Total weight	490	490	490	490	490	490	490	490	495

#### 4.13. Pre-compression parameter of powder blend:

Powder blend were evaluated for various pre-compression parameters such as Angle of repose, Loosed bulk density (LBD), Tapped bulk density (TBD), Compressibility index and Hausner's ratio. The blends were compressed using a single-punch tablet compression machine using 8.0 mm standard concave punch, and their physical parameters were evaluated, such as the average weight, thickness, hardness and friability.

#### 4.14. Evaluation parameters of tablets:

Evaluation parameters for Floating drug delivery system of Pregabalin are shown in Table 09.

**Table 9:** Evaluation parameters applicable for Mucoadhesive and Floating drug delivery system of Pregabalin

Sr. No	Evaluation parameters
1	Weight Variation test
2	Thickness
3	Hardness
4	Friability
5	Drug content
6	Swelling index
7	In vitro buoyancy study
8	Kinetic modeling of drug release
9	In vitro stability study

**a) Weight Variation test**

Twenty tablets were taken from each formulation and weighed individually to check for weight variation (Table 10). Calculated average weight and compared the individual tablet weight to the average.

**Table 10:** Weight variation tolerances for tablets

Average weight of tablets (mg)	Maximum % difference allowed
80 or less	10
80 – 250	7.5
More than 250	5

**b) Thickness:** Thickness of tablets was measured by using digital Vernier caliper.

**c) Hardness:** Tablets were selected at random from individual formulations and hardness was measured and expressed in Kg/cm<sup>2</sup> or Newton's (N).

**d) Friability:** Twenty tablets were randomly selected and placed in the drum of a tablet friability test apparatus. The drum was adjusted to rotate 100 times in 4 min. The tablets were removed, dedusted and accurately weighed. The percent weight loss was calculated. Results are expressed as mean values  $\pm$  SD.

$$\text{Friability (\%)} = \frac{\text{Initial weight} - \text{Final weight}}{\text{Initial weight}} \times 100 \quad (6)$$

**I. In vitro study****a) Drug content**

Accurately weighed and powdered 20 tablets, weighed accurate quantity of the powder equivalent to 330 mg of Pregabalin into 100 ml of volumetric flask, add 30 ml of Acetonitrile, mix and sonicate for 5 minutes to dissolve and dilute to volume with pH 6.5, buffer solution. Filter through 0.45  $\mu$ l filter. Dilute 5 ml to 50 ml with mobile phase (Acetonitrile: pH 6.5 buffer). Record the chromatogram and measure the peak responses at 226 nm and calculate the content of Pregabalin in the sample.

**b) Swelling study**

The tablets were weighed individually (as W<sub>1</sub>), placed separately in glass beaker containing 200 ml of 0.1 N HCl and incubated at  $37 \pm 1$  °C. The mucoadhesive tablets were removed from the beakers at 1-hour intervals (over a total of 12 h), and the liquid was removed carefully from the surface using paper. The swollen tablets were then weighed (W<sub>2</sub>). The swelling index (SI) was calculated using the following formula.

$$\% \text{ Swelling Index} = (W_2 - W_1) / W_1 \times 100$$

Where W1- Initial weight of tablet, W2- Weight of the swollen tablet.

### c) *In vitro* buoyancy studies

The *in vitro* buoyancy was determined by buoyancy lag time. The time taken for the tablet to rise to the surface and float was taken as floating lag time. The test was performed by placing each of the tablets in a 250 ml beaker containing 200 ml of 0.1 N HCl, pH 1.2 maintained at  $37 \pm 0.5$  °C in a water bath.

### d) *In vitro* drug released study

The drug release of various formulations (X1-X9) was studied *in vitro* using USP type II apparatus set at 100 rpm. A buffer medium with pH 3.0 (900 ml) at  $37.5 \pm 0.5$  °C was used. A 10 ml sample was withdrawn at 1, 2, 4, 6, 8, 10 h time intervals over a period of 12 h and replaced with the same dissolution media. The withdrawn samples were analyzed using UV Spectrophotometry at 226 nm. Kinetic modeling of drug release. The drug released profile of all the batches was analyzed using the zero order, first order, Higuchi, Hixon-crowell, Korsmeyer's Peppas model was selected to perform kinetic modeling of the drug release. A criterion for selecting the most appropriate model was based on high regression coefficient value.

## 5. Results and Discussion

### A) Preformulation Study

#### Confirmation of drug:

Confirmation of drug was carried out by following methods.

#### 5.1. FTIR Spectroscopy

The IR spectrum was obtained in the solid state as potassium bromide dispersion. The IR spectrum of Pregabalin is presented in Fig 12. Observed peaks are shown in Table 11.

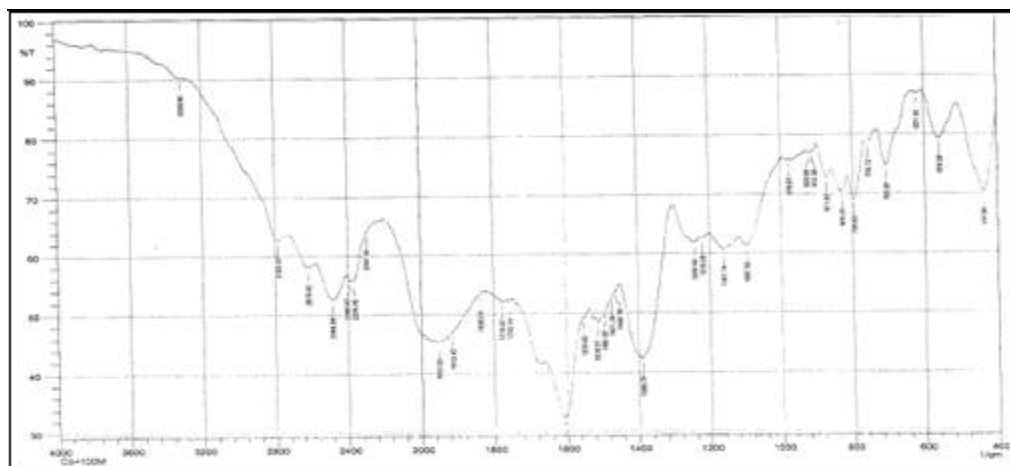


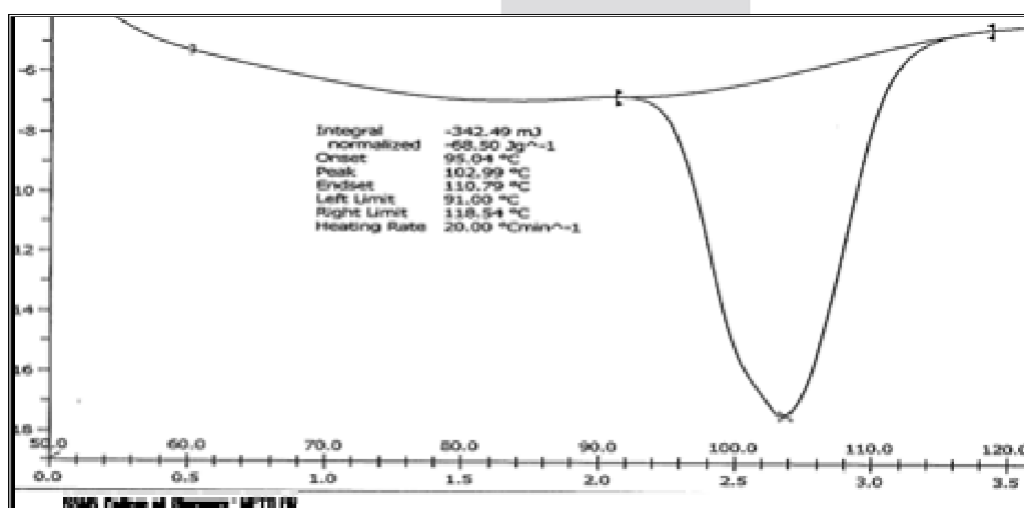
Fig: 12. IR spectrum of Pregabalin

**Table 11:** Principal peak and functional group present in IR spectrum of Pregabalin

Sr. No	Peak observed (cm <sup>-1</sup> )	Functional group
1.	2937.04	C-H Stretching (Aliphatic)
2.	2984.39	C-H Stretching (Aromatic)
3.	3330.81	N-H Stretching
4.	1618.01	N-H Bending
5.	1638.04	C=N Stretching
6.	1074.15,1099.46	C-O Stretching
7.	1761.84	C= O Stretching
8.	674.20	C-S-C Stretching
9.	1274.25	C-N Stretching
10.	1375.64	C-H Bending

### 5.2.DSC study:

Pregabalin was confirmed by differential scanning calorimetry (DSC) at scan rate of 10 °C / min. The DSC thermogram of Pregabalin (Fig. 13) exhibited a single sharp endothermic peak at 98.79 °C and 102.99 °C respectively, related to its melting transition temperature. Okonogi and Puttipatkhachorn., 2006)

**Fig. 13:** DSC thermogram of Pregabalin

### 5.3. Melting point determination

The melting point of Pregabalin was confirmed by using melting point apparatus. The melting point of Pregabalin was found to be in the range of 98.04 -102.99 °C

## 5.4. Solubility Study

Results of solubility studies are shown in Table 24.

**Table 12:** Solubility study of Pregabalin and Pregabalin in different solvent

Sr. No	Solvent	Solubility (mg/ml)
1.	0.1N HCl (pH 1.2)	5.60
2.	Glycine buffer (pH 3.0)	6.10
3.	pH 4.5	0.40
4.	pH 6.8	0.37

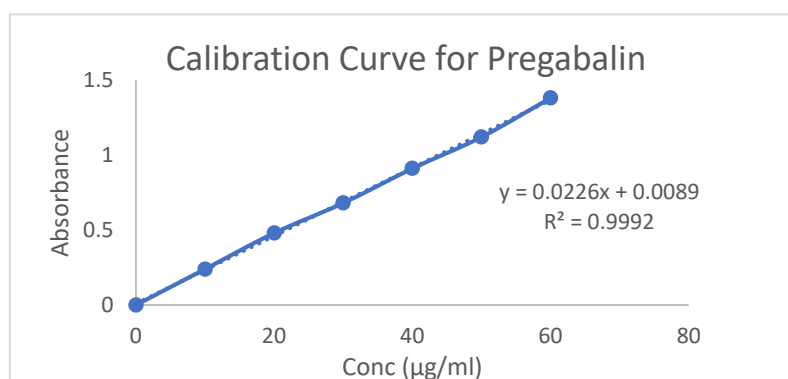
### a) Standard calibration curve:

#### Standard calibration curve of Pregabalin in pH 3.0:

Calibration curve of Pregabalin in glycine buffer pH 3.0 was studied; plots of area verses concentration was found to be linear between the range of 10 to 60 µg/ml. The  $r^2$  value of the calibration curve was found to be 0.999. Results of standard calibration curve of Pregabalin in glycine buffer (pH 3) are shown in Fig. 14 and Table 13.

**Table 13: Calibration Curve of Pregabalin**

SL.No	Concentration (µg/ml)	Absorbance
1	10	0.24
2	20	0.48
3	30	0.68
4	40	0.91
5	50	1.12
6	60	1.38



**Fig 14: Calibration Curve of Pregabalin**

**B) Evaluation of precompression parameters of drug, polymers and excipients**

Drug, polymers and excipient were characterized for their physical properties such as angle of repose, density, compressibility, Hausner's ratio and given in Table 14.

**Table 14:** Evaluation of precompression parameters of drug, polymers and excipients

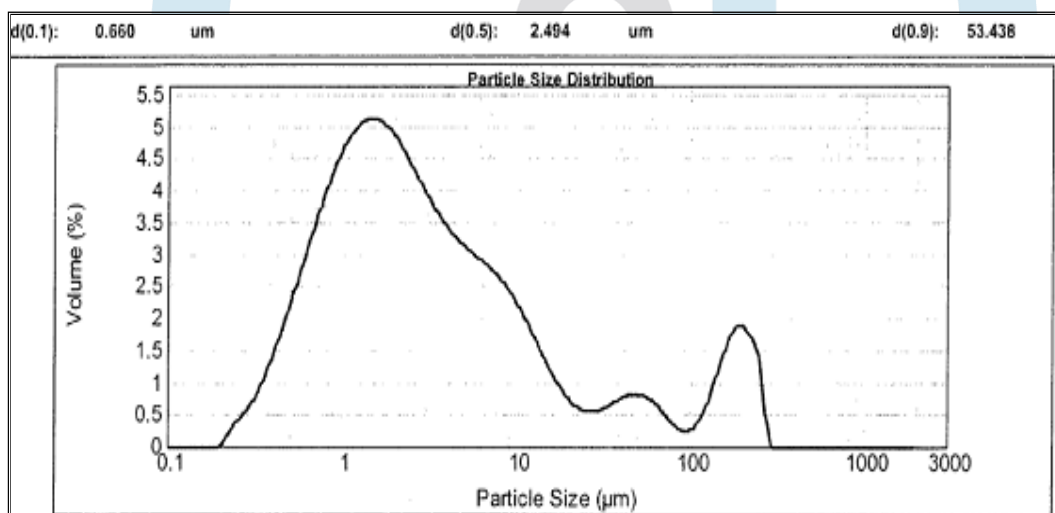
Ingredients	Angle of repose ( $\theta$ )	Bulk density gm/ml	Tapped density (gm/ml)	Hausner's ratio	Compressibility index (%)
Pregabalin	36.00 $\pm$ 1.32	0.416 $\pm$ 0.015	0.545 $\pm$ 0.016	1.18 $\pm$ 0.01	18.17 $\pm$ 0.15
HPMC K100 LV	30.00 $\pm$ 1.20	0.220 $\pm$ 0.003	0.260 $\pm$ 0.004	1.18 $\pm$ 0.030	15.38 $\pm$ 0.54
HPMC K4M	30.00 $\pm$ 1.30	0.240 $\pm$ 0.004	0.330 $\pm$ 0.006	1.37 $\pm$ 0.026	27.27 $\pm$ 1.16
MCC KG 100	35.00 $\pm$ 1.10	0.290 $\pm$ 0.006	0.420 $\pm$ 0.003	1.45 $\pm$ 0.053	19.41 $\pm$ 1.28
Sodium lauryl sulphate	28.00 $\pm$ 1.30	1.500 $\pm$ 0.006	2.350 $\pm$ 0.028	1.56 $\pm$ 0.025	36.59 $\pm$ 1.25
Sodium bicarbonate	37.00 $\pm$ 2.00	1.100 $\pm$ 0.035	1.760 $\pm$ 0.022	1.60 $\pm$ 0.025	37.50 $\pm$ 1.22
Citric acid	28.00 $\pm$ 1.5	0.630 $\pm$ 0.01	1.000 $\pm$ 0.01	1.60 $\pm$ 0.06	37.5 $\pm$ 1.30

	0	50	55	3	
Magnesium	30.	0.4	0.6	1.5	33.33
stearate	00±	00	00	0±	±1.20
	1.1	±0.	±0.	0.5	
	2	07	06	0	

\*All the values are mean  $\pm$  SD of three determinations.

### 5.3. Particle size determination:

Particle size determination of Pregabalin was determined using dry method by Malvern technique and given in Fig 15.



**Fig. 15:** Particle size distribution of Pregabalin by Malvern technique.

D (0.9): 53.438  $\mu\text{m}$  (90 % the particles were 53.438  $\mu\text{m}$  or above)

D (0.5): 2.494 (50 the particles were 2.494  $\mu\text{m}$  or above)

D (0.1): 0.660  $\mu\text{m}$  (10 % of the particles were 0.660  $\mu\text{m}$  or above)

### 5.4. Drug excipients compatibility study:

The drug excipients interaction study was carried out by using Fourier Transform Infrared spectroscopy and differential scanning calorimetry (DSC). In this study thermogram of pure drug, drug with polymer and mixtures of drug with excipients were taken and given in Fig16-18. The FTIR spectrum and DSC thermogram of alone drug is shown below.

### 5.5. DSC study of Pregabalin physical mixture:

The drug, drug-excipients physical mixture studies reveal that there were no significant change in position of peak in thermogram of drug, drug-excipients was recorded. The DSC thermogram of Pregabalin exhibited a single sharp endothermic peak at 98.79 °C related to its melting transition temperature shown in Fig. 18a and drug excipients physical mixture shows melting endothermic peak of Pregabalin at 100.92 °C shown in Fig.18 b-h. From drug excipients compatibility study, it was concluded that the given drug was compatible with all the excipients and it was confirmed by DSC study.

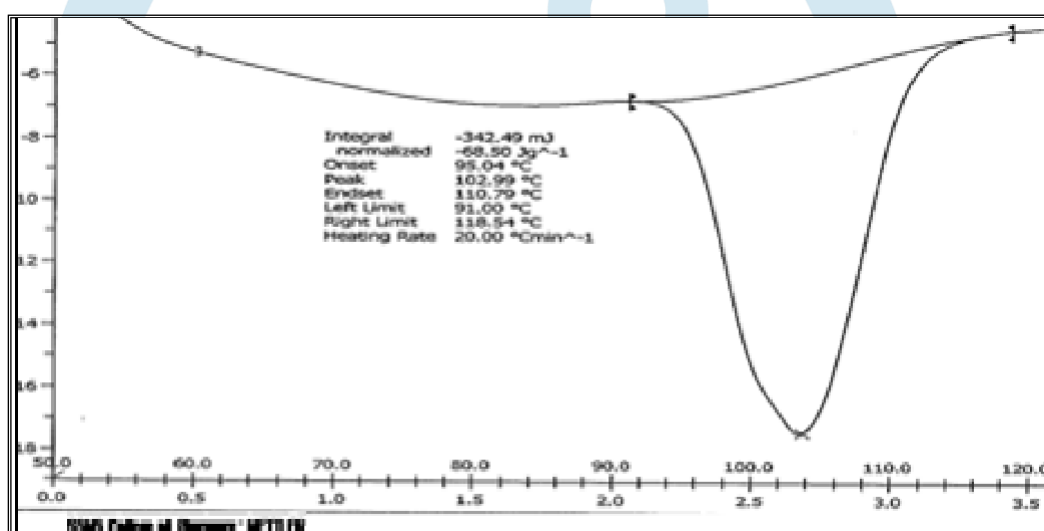


Fig. 16: DSC thermogram of Pregabalin.

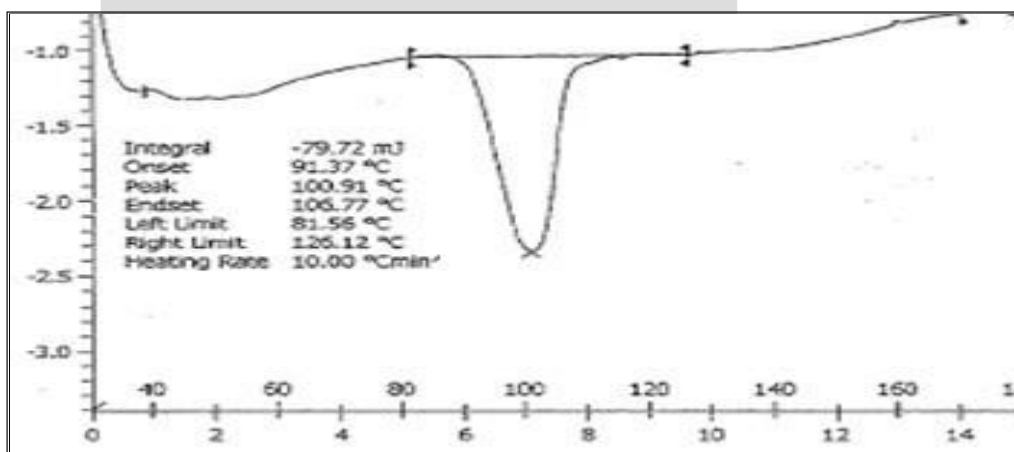


Fig. 17: DSC thermogram of Pregabalin with excipients mixture.

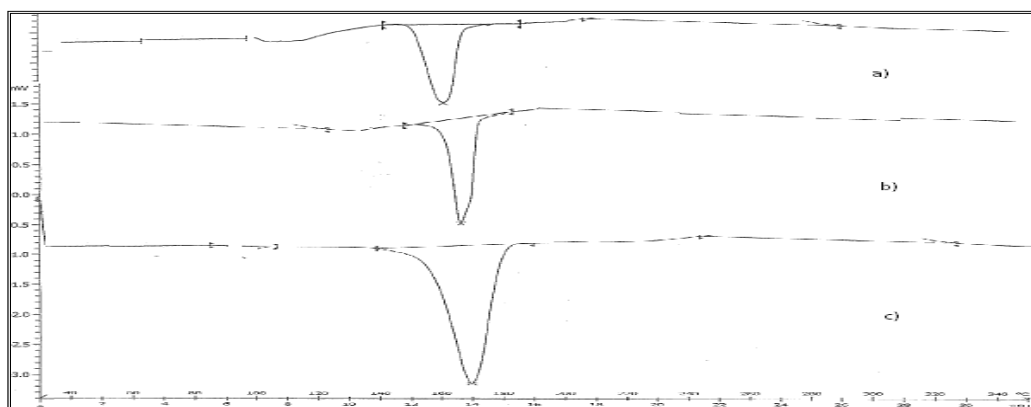


Fig. 18: DSC thermogram of a) Pregabalin (b) Pregabalin with HPMC K4M (c) Pregabalin with



### C) Evaluation of precompression parameters of powder blend

The powder blend of various formulations shows good flow property. Results are shown in Table 15. Results of various formulations revealed that the powder blend can be directly compressed into tablets.

**Table 15:** Evaluation of pre-compression parameters of Floating tablets of Pregabalin (X1-X9)

Parameters	X1	X2	X3	X4	X5	X6	X7	X8	X9
LOD (%)*	1.68±0.67	1.72±0.88	1.89±0.94	1.69±0.78	1.80±0.88	1.91±0.96	1.79±0.075	1.94±0.57	1.83±0.94
Bulk density (gm/ml)*	0.205±0.05	0.215±0.08	0.202±0.07	0.207±0.06	0.210±0.04	0.199±0.08	0.215±0.08	0.198±0.06	0.201±0.03
Tapped density (gm/ml)*	0.249±0.04	0.250±0.09	0.245±0.08	0.239±0.02	0.242±0.08	0.237±0.09	0.247±0.08	0.239±0.09	0.237±0.07
Carr's compressibility index (%)*	17.67±1.98	14.00±2.15	17.55±2.32	13.39±2.11	13.22±1.80	16.03±1.98	12.95±2.11	17.15±2.15	15.18±2.50
Hausner's ratio*	1.214±0.24	1.162±0.3	1.212±0.35	1.150±0.29	1.157±0.27	1.190±0.24	1.195±0.28	1.200±0.45	1.179±0.47
Angle of repose(Ø)	41.50±2.00	41.30±2.50	36.61±1.85	35.68±1.54	38.32±1.66	34.68±1.68	42.69±2.50	42.51±2.11	40.63±2.31

### D) Evaluation of Post Compression Parameters for Pregabalin Tablets

Physicochemical parameters of the formulations X1-X9 were within the acceptance limit. All the batches passed the Pharmacopoeial limits. The drug content was found to be within a narrow range as specified in pharmacopoeia (90-110 %) in all the formulations. Almost all the batches showed uniform thickness and drug content. All batches passed weight variation test and found to be within range ( $\pm 5$  %) and friability was less than 1.0 %, it indicates that tablet surfaces are strong enough to withstand mechanical shock or attrition during storage, transportation and until they are consumed. post compression parameters, results are shown in Table 16.

**Table 16:** Physicochemical characterization of Floating tablets of Pregabalin (X1-X9)

Parameters	X1	X2	X3	X4	X5	X6	X7	X8	X9
Average weight (mg)*	490± 3	490± 3	490± 3	490± 3	490± 3	490± 3	490± 3	490± 3	495± 3
Thickness (mm)*	5.83	5.82	5.82	5.83	5.84	5.84	5.83	5.8	5.86
Hardness (kg/cm <sup>2</sup> )*	4-5	4-5	4-5	4-5	4-5	4-5	4-5	4-5	4-5
Friability (%)	0.25	0.43	0.33	0.46	0.56	0.49	0.51	0.46	0.52
Buoyancy lag time (sec)*	21 ± 3	23 ± 3	20 ± 3	25 ± 3	27 ± 3	26 ± 3	29 ± 3	30 ± 3	35 ± 3
Total buoyancy time (h)	12	12	12	8	12	10	12	12	12
Drug content (%)*	99.27 ± 1.58	98.64 ± 1.58	99.00 ± 1.58	99.71 ± 1.58	100.11 ± 1.58	99.51 ± 1.58	100.1 ± 1.58	100.34 ± 1.58	100.15 ± 1.58

\*All values are mean ± SD of three determinations.

## 5.6. Swelling study:

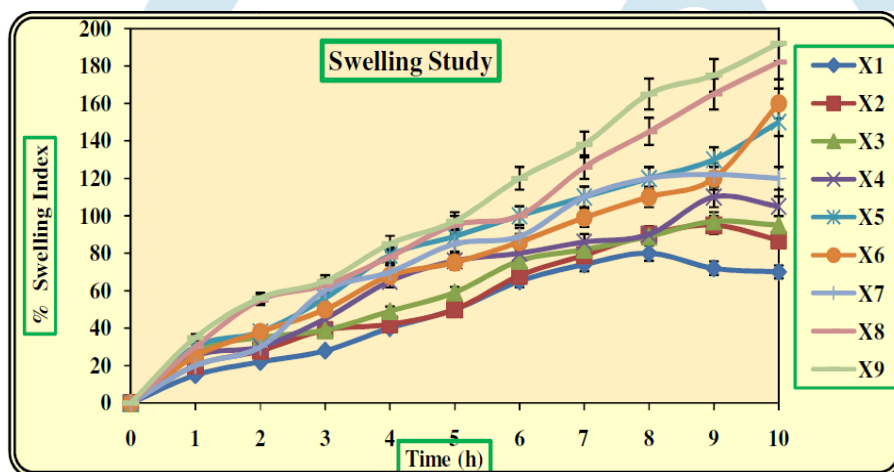
Swelling is also a very important factor to ensure drug dissolution of the formulation. The hydration ability of the formulation influences; (i) tablet buoyancy (ii) adhesion ability of swellable polymers and (iii) drug release kinetics. Pregabalin composed of polymeric matrices build a gel layer around the tablet core when they come in contact with water. The ability of hydrogel to absorb water is due to the presence of hydrophilic groups. The ability of hydrogel to absorb water is due to the presence of hydrophilic groups. The hydration of these functional groups results in water entry into the polymer network leading to expansion and consequently an ordering of the polymer chains. The hydration of these functional groups results in water entry into the polymer network leading to expansion and consequently an ordering of the polymer chains.

### a) Swelling study (for floating gastroretentive formulation)

The floating tablets of Pregabalin composed of polymeric matrices build a gel layer around the

tablet core when they come in contact with water. This gel layer governs the drug released from the matrix tablet. The floating tablets containing HPMC K4M with HPMC K100 LV (X7) showed less swelling index at the

beginning but was found thick gel formation at the end of 8 h also maintains their matrix integrity up to 6 -7 h. These results suggest that the dried particles may swell in the stomach; the particles may begin to swell more and behave as matrices for controlled release of incorporated drug.



**Fig. 22: Swelling index of Pregabalin floating tablets (X1 to X9)**

#### **In vitro buoyancy studies (For floating gastroretentive drug delivery system):**

This test was only performed to check the floating behavior of floating formulations. The buoyancy of floating tablet was studied at  $37 \pm 0.5$  °C in 200 ml of 1.2 pH buffer (Simulated gastric fluid without pepsin). The buoyancy lag time was measured by using stop watch and total floating time was observed visually until they are consumed. Floating lag time was observed less than 50 sec for all batches. Total floating time was observed more than 12 h.

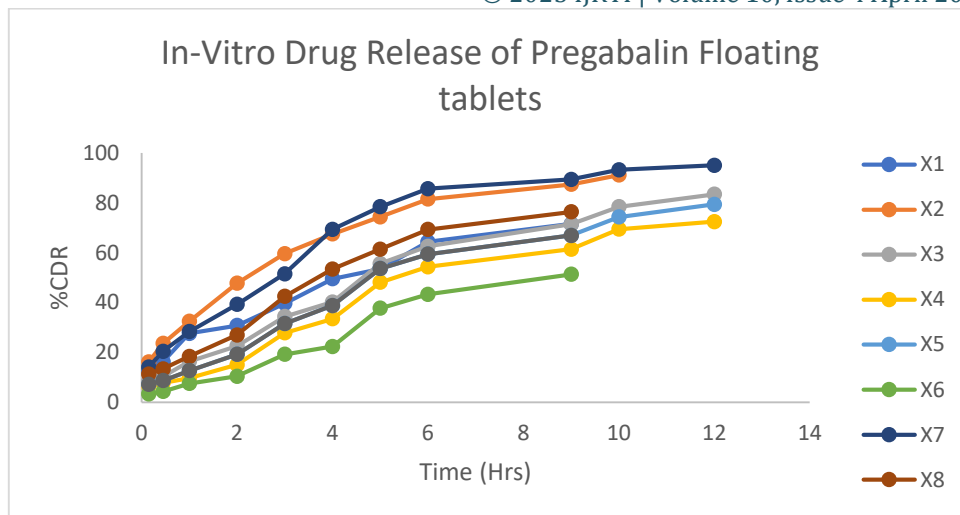
#### **5.7. In vitro drug released studies:**

##### **In vitro drug released for gastroretentive drug delivery system:**

In order to evaluate different hydrophilic matrixing polymers used to prepare Floating Gastroretentive tablets polymers like HPMC K4M, in combination with low viscosity polymer HPMC K100 LV were selected for floating tablets of Pregabalin and their individual drug released profile was evaluated. The gastroretentive tablets with formulations X1 to X9, containing combinations of HPMC K4M and HPMC K100 LV in different ratios exhibited cumulative percent drug release values of 71.52, 91.12, 83.43, 72.43, 79.38, 51.32, 95.06, 76.36 and 66.89, respectively. In the presence of HPMC K4M, HPMC K100 LV produces a firm gel that entraps the gas for a longer time and delays the release of the drug.

X1	X2	X3	X4	X5	X6	X7	X8
12.71	16.2	8.28	6.37	7.17	3.33	14.13	11.1
16.2	23.56	10.25	7.78	8.67	4.31	20.4	13.1
27.59	32.45	16.36	9.66	12.62	7.52	28.3	18.1
30.75	47.68	22.52	15.05	19.22	10.38	39.22	26.1
39.63	59.62	34.37	27.79	31.52	19.19	51.48	42.1
49.52	67.52	40.19	33.47	38.78	22.33	69.38	53.1
53.52	74.35	55.58	48.07	53.64	37.67	78.4	61.1
64.35	81.52	62.54	54.35	59.4	43.3	85.65	69.1
71.52	87.41	71.42	61.42	66.89	51.32	89.41	76.1
	91.12	78.42	69.44	74.3		93.25	
		83.43	72.43	79.38		95.06	

**Table 17: In-Vitro Drug Release of Pregabalin Floating tablets**



**Fig: 23: In vitro Drug released of Pregabalin floating tablets (X1 to X9).**

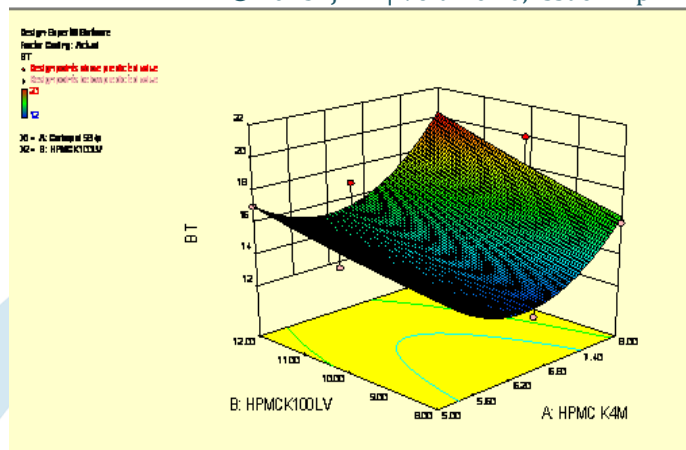
### 5.7. Kinetic modeling of drug release for Floating Gastroretentive tablets:

The data obtained from the in vitro drug released studies of formulation X1-X9, were fitted to zero-order, first-order, Higuchi Korsmeyer Peppas equations, and the data were analyzed (Table 18). The  $r^2$  value of the optimized formulation X7 was found 0.98. The  $n$  values of the optimized formulation (X7) was found to be 0.547, which fall in the range  $0.35 < n < 0.50$  and  $k$  value was 17.61 with good floating properties. The value of the diffusion exponent indicates that the drug release follows non-Fickian release mechanism.

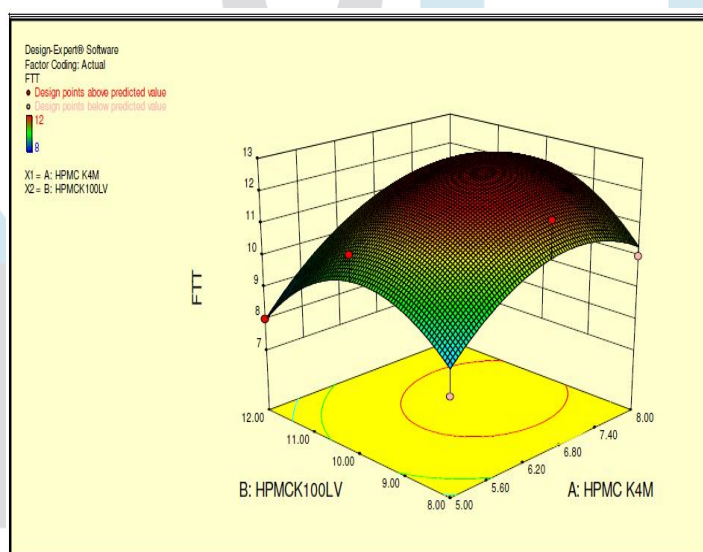
**Table 18: Kinetic parameters of Pregabalin tablets (X1-X9)**

Batch Code	Zero order ( $R^2$ )	First order ( $R^2$ )	Higuchi ( $R^2$ )	Korsmeyer – Peppas ( $R^2$ )	n (Release exponent)	Hixon-Crowel
X1	0.908	0.973	0.982	0.989	0.511	0.848
X2	0.940	0.949	0.980	0.989	0.548	0.733
X3	0.908	0.89	0.952	0.989	0.525	0.876
X4	0.905	0.878	0.887	0.989	0.446	0.705
X5	0.938	0.926	0.951	0.989	0.467	0.893
X6	0.952	0.910	0.971	0.989	0.529	0.730
X7	0.982	0.977	0.976	0.989	0.547	0.850
X8	0.919	0.927	0.946	0.989	0.562	0.890
X9	0.959	0.895	0.987	0.989	0.458	0.843





**Fig. 25:** Response surface plot showing % BLT of formulation X7.



**Fig. 26:** Response surface plot showing % FTT of formulation X7.

## 6. Conclusion:

In **conclusion**, the tablets containing HPMC K4M with HPMC K100 LV (X7) had a short buoyancy lag time, a total floating time of more than 10 h and sustained release up to 12 h. This novel gastro retentive dosage form could be fascinating for enhancement of bioavailability and the stomach specific delivery of pregabalin. From the above study it could be concluded that floating gastroretentive drug delivery system is most stable system. The observed independent variables were found to be very close to predicted values of most satisfactory formulation which demonstrates the feasibility of the optimization procedure in successful development of Pregabalin tablets.

## 7. Bibliography:

1. Arora S, Ali J, Ahuja A, Khar RK, Baboota S. Floating drug delivery systems: A review. AAPS PharmSciTech 2005; 6:E372-90.
2. Atyabi F, Sharma H, Mohammad H, Fell J. *In vitro* evaluation of a novel gastro retentive formulation

based on ion exchange resins. *J ControlRelease* 1996; 42:105-13.

3.Chawla, G., Bansal, A., Gupta, P., Koradia, V., 2003. Gastro retention a means to address regional variability in intestinal drug absorption. *Pharmaceutical technology* 07, 50-68.

4.Basak S.C., Rao K.N., Manavalan R., Rao P.R. Development and in vitro evaluation of an oral floating matrix tablet formulation of ciprofloxacin. *Indian J. Pharm. Sci.* 2004, 66: 313–16.

5.Baumgartner, S., Kristl, J., Vercer, F., Vodopiec, P., Zorko, B., 2000. Optimization of floating matrix tablets and evaluation of their gastric residence time. *Int. J. Pharm.* 195, 125-35.

6.Bhupesh D, Raghuram C. An open-label randomized cross-over bioequivalence study of lafutidine 10 mg under fasting condition. *World Journal of Gastrointestinal Pharmacology and Therapeutics.* 2010; 1:5:112–18.

7.Caldwell L. Gardner R., Cargill R. (1988a). Drug delivery device which can be retained in the stomach for a controlled period of times. *US patents, 30th August* 1988; 4,767,627.

8.Caldwell L., Gardner R., et al. Drug delivery device which can be retained in the stomach for a controlled period of times. *US patents, 5th April* 1988; 4,735,804.

9.Chary R., Rao Y., Formulation Evaluation of Methocel K15 M Bioadhesive matrix tablet. *Drug Dev Ind Pharm* 2000; 26:901-6.

10.Chavanpatil M.D., Jain P., Chaudhari S., Shear R., Vavia P.R. Novel sustained release, swellable bioadhesive gastroretentive drug delivery system for ofloxacin. *Int. J. Pharm.* 2006, 316: 89–92.

11.Chien Y, Novel drug delivery systems. 2nd edition, Marcel Dekker Inc., NY, 1992; 171-76.

12.Cobby J., Mayersohn M., Walker G.C. Influence of shape factors on kinetics of drug release from matrix tablets. *J. Pharma. Sci.* 1974, 63: 732–37.

13.Desai S, Bolton S. A floating controlled-release drug delivery system: *In vitro–in vivo* evaluation. *Pharm Res* 1993; 10:1321-5.

14.Deshpande A., Rhodes C., Controlled released drug delivery systems for prolonged gastric residence: an over view. *Drug Dev. Ind. Pharm*, 1996; 22:531- 39.

15.Design Expert® software version 8.0.3.1 Operation Manual (2010)

16.Dollery C. Therapeutic Drugs. Edinburgh, Scotl: Churchil Livingstone; 1999:C113YC117.

17.Dorozynski P, Jachowicz R, Kulinowski P, Kwieciński S, Szybiński K, Skórka T, *et al.* The macromolecular polymers for the preparation of hydrodynamically balanced systems – Methods of evaluation. *Drug Dev.Ind Pharm* 2004; 30:947-57.

18.Dyer J., ed. Applications of Absorption Spectroscopy of Organic Compounds. New Delhi: Prentice-Hall of India Pvt. Ltd. 1<sup>st</sup> edition. 1997:33

19.Gandhi R.B., Robinson J.R., Bioadhesion in drug delivery. *Ind. J. Pharm. Sci* 1998 50(3):145-52.

20.Garg R, Gupta GD. Progress in controlled gastro retentive delivery systems. *Trop. J Pharm Res* 2008; 7(3): 1055-66.

21.Gershon, S., Pader M., et al. Cosmetics Science and Technology, Wiley- Interstice, New York, 1972, 423

22.Gibaldi M, Feldman S. Establishment of sink conditions in dissolution rate determinations. Theoretical considerations and application to nondisintegrating dosage forms. *J Pharm Sci* 1967;

56:1238-42.

23.Gowda D.V., Raghunandan V., Pai V.K., Lakshmi C.R, Khan M.S., Bhat S. Development and evaluation of gastroretentive floating tablets of anti- hyperlipidemic. *Int. J. Drug Delivery* 2012, 4: 175-83.

24.Gupta Amit M., Belgamwar Aarti V., Wake Prashant S., Rathi Trivesh P., Mundhada D.R. Design and development of hydrodynamically balanced tablet of itopride. *J. Chem. Pharm. Res.* 2011, 3(6): 856-64.

25.Higuchi T. Mechanism of sustained-action medication. Theoretical analysis of rate of release of solid drugs dispersed in solid matrices. *J Pharm Sci* 1963; 52:1145-9.26.Hixson AW, Crowell JH. Dependence of reaction velocity upon surface agitation. *IndEngchem* 1931; 23:923-93.

27.Iannuccelli V., Coppi C., Bernabei M, et al. (1998). Air compartment multi unit systems for prolong gastric residence, Part I: Formulation study. *Int.J.Pharm.* 1998:174:47-54.

28.Ichikawa T, Ishihara K, Saigenji K, Hotta K. Lafutidine induced stimulation of mucin biosynthesis mediated by nitric oxide is limited to the surface mucous cells of rat gastric oxyntic mucosa. *Life Sci* 1998; 62:PL259-64.

29.Ikawa K, Shimatani T, Hayato S, Morikawa N, Tazuma S. Pharmacokinetic and pharmacodynamic properties of lafutidine after postprandial oral administration in healthy subjects: Comparison with famotidine. *Biol Pharm Bull* 2007; 30:1003-6.

30.Inaba N, Shibata M, Onodera S, Tanaka M, Suzuki T, Yamaura T, et al. Studies on histamine H2 receptor antagonistic property of FRG8813, a novel antiulcer drug. *Nihon Yakurigaku Zasshi* 1995; 105:231-41.

31.International Conference on Harmonization steering committee, Q1A- Stability testing of new drug substances and products; 1999.

32.Kakumanu V.K., Arora V.K., Bansal A.K. Gastro-retentive dosage form for improving bioavailability of cefpodoxime proxetil in rats. *Yakugakud Zasshi Pharm.* 2008, 3: 439-45.

33.Kato S, Tanaka A, Kunikata T, Umeda M, Takeuchi K. Protective effect of lafutidine against indomethacin-induced intestinal ulceration in rats: Relation to capsaicin sensitive sensory neurons. *Digestion* 2000; 61:39-46.

34.Kiortsis S, Kachrimanis K, Broussali T and Malamataris S. Drug release from tableted wet granulations comprising cellulosic (HPMC or HPC) and hydrophobic component. *Eur. J. Pharm. Biopharm* 2005; 59: 73-83.

35.Klausener E.A., Lavy E., Friedman M., Hoffman A. Expandable gastro retentive dosage form. *J. Control. Release* 2003, 90: 143-62.

36.Korsmeyer R, Gurny R, Doelker E, Buri P and Peppas N. Mechanisms of solute release from porous hydrophilic polymers. *Int J Pharm* 1983; 15:25–35.

37.Lachman L, Hebert AL, Joseph LK. Theory and Practice of Pharmacy, 3rd edition, Varghese Publication House; 1987, pp. 430-34.

38.Lehr CM. Bioadhesion technologies for the delivery of peptide and protein drugs to the gastrointestinal tract. *Crit.Rev.Ther.Drug Carrier Syst.*1994;11:119-6.39.Mathews BR. Regulatory

aspects of stability testing in Europe. *Drug Dev. Ind. Pharm.* 1999; 25:831-56.

40.Moes A.J. Gastroretentive dosage forms. *Rev. Ther. Drug Carr. Syst.* 1993; 10:143-95.

41.Nur A., Zhang J. Captopril floating bioadhesive tablets: designed release kinetics.

*Drug Dev. Ind. Pharm.* 2000, 26: 965-69.

42.Onodera S, Shibata M, Tanaka M, Inaba N, Arai Y, Aoyama M, *et al.* Gastroprotective mechanism of lafutidine, a novel anti-ulcer drug with histamine H<sub>2</sub>-receptor antagonistic activity. *Arzneimittel for schung* 1999; 49:519-26.

43.Onodera S, Shibata M, Tanaka M, Inaba N, Yamaura T, Ohnishi H. Gastroprotective activity of FRG-8813, a novel histamine H<sub>2</sub>-receptor antagonist, in rats. *Jpn J Pharmacol* 1995; 68:161-73.

44.Peppas N.A. Analysis of Fickian and non-Fickian drug release from polymers. *Pharm ActaHelv* 1985; 60:110-11.

45.Reddy L.H., Murthy R.S. Floating dosage system in drug delivery. *Crit. Rev. Ther. Drug Carrier Syst.* 2002, 19(6): 553-85.

46.Rosa M, Zia H, Rhodes T. Dosing and testing *in vitro* of a bioadhesive and floating drug delivery system for oral application. *Int J Pharm* 1994; 105:65-70.

47.Rouge N., Allemann E., Gex-Fabry M, *et al.* (1998). Comparative pharmacokinetic study of a floating multiple-unit capsule, a high-density multiple- unit capsule an immediate-release tablet containing 25 mg Atenolol. *Pharmaceutical Acta Helvetiae* 1998; 73:81-87.

48.Saathoff N., Lode H., Neider K., *et al.* Pharmacokinetics of Cefpodoxime Proxetil interactions with an antacid an H receptor antagonist. *Antimicrobial Agents, Chemotherapy.* 1992; 36:796Y800.

49.Salve P. S. Effect of excipients and processing parameters on floating characteristics of hydrodynamically balanced system for Diltiazem hydrochloride. *Asian J. Res. Pharm. Sci.* 2011, 1 (4): 97-99.

50.Santus G., Lazzarini G., Bottoni G., Sandefer E,P., Page R,C., Doll W, J., *et al.* An *in vitro* *in vivo* investigation of oral bioadhesive controlled release furosemide formulations. *Eur. J. Pharma. Biopharm.* 1997, 44: 39-52.

51.Seth P.R., Tossounian J. The hydrodynamically balanced system: a novel drug delivery system for oral use. *Drug Dev. Ind. Pharm.* 1984, 10: 313-39.

52.Shah S.U., Shah K.U. and Rehman A. Investigating the *in vitro* drug release kinetics from controlled release diclofenac potassium–ethocel matrix tablets and the influence of co-excipients on drug release patterns. *Pak. J. Pharm. Sci.* 2011, 24 (2): 183-92.

53.Singh B., Kim K., Floating drug delivery systems: an approach to oral controlled drug delivery via gastric retention. *J.Control Release*, 2000: 63:3, 235-59.

54.Streobel A., Siepmann J., Bodmeier R. (2006).Gastroretentive drug delivery systems. *Expert Opinion on, Drug Delivery.* 2006; 3(2):217-33.

55.Suvarna K, Manisha S, Sugandha V. Development and validation of an UV spectrophotometric method for estimation of Lafutidine in bulk and tablet dosage form contemporary investigation and observation in pharmacy 2012; 1:1; 5-8

56.Tadros, M.I. Controlled-release effervescent floating matrix tablets of ciprofloxacin hydrochloride:

development, optimization and in vitro–in vivo evaluation in healthy human volunteers. *Eur. J. Pharm. Biopharm.* 2010, 74 (2): 332-39.

57. Todd W.M. Cefpodoxime proxetil: a comprehensive review. *Int. J. Antimicrob. Agents* 1994, 4: 37-62.

58. Wagner J. Interpretation of percent dissolved-time plots derived from in vitro testing of conventional tablets, capsules. *J. Pharm. Sci.* 1969, 58: 1253-57.

59. Venkatasubbu G.D., Ramasamy S., Ramakrishnan V., Kumar J. Nanocrystalline hydroxyapatite and zinc-doped hydroxyapatite as carrier material for controlled delivery of ciprofloxacin. *Biotech* 2003, 1(3): 173-86.

60. Whitehead L, Fell JT, Collett JH, Sharma HL, Smith A. Floating dosage forms: An *in vivo* study demonstrating prolonged gastric retention. *J Control Release* 1998; 55:3-12.

[www.Rxlist.com/Reglan](http://www.Rxlist.com/Reglan)

61. Yamagishi H, Koike T, Ohara S, Horii T, Kikuchi R, Kobayashi S, *et al.* Stronger inhibition of gastric acid secretion by lafutidine, a novel H<sub>2</sub> receptor antagonist, than by the proton pump inhibitor Lansoprazole. *World J Gastroenterol* 2008; 14:2406-10.

62. Yie Chein., oral drug delivery and delivery systems. *Novel drug delivery systems, Marcel Dekker* 1992; 139-96.

IJRTI